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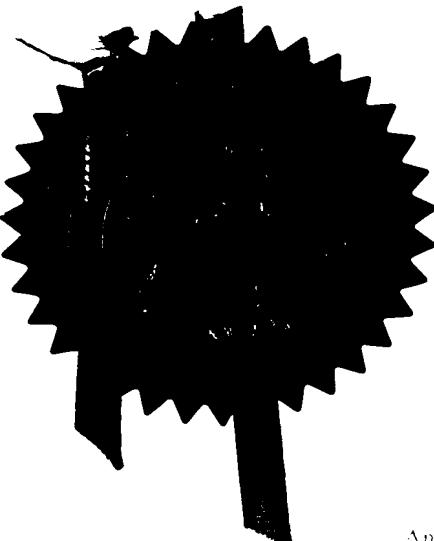
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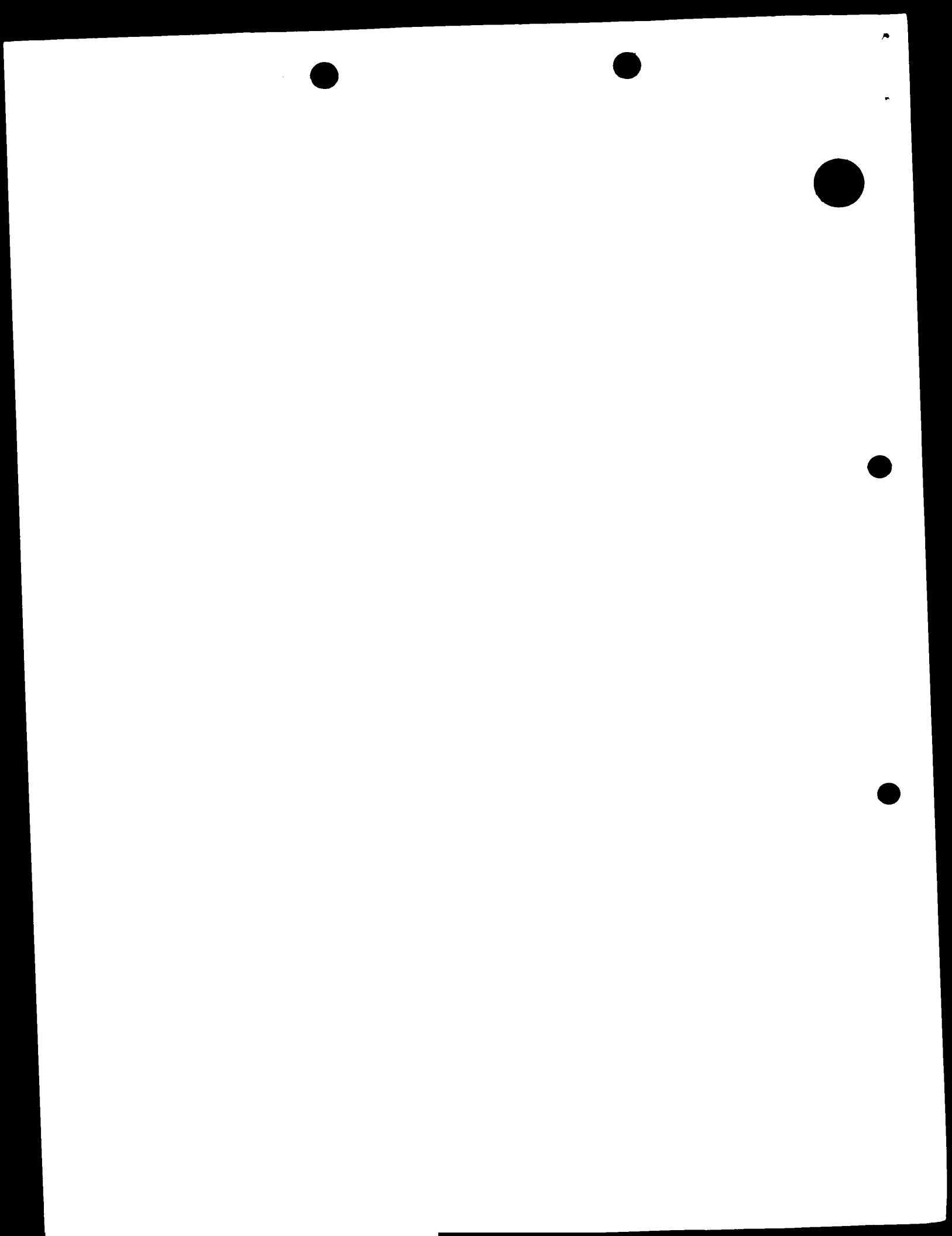


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Torsana Biosensor A/S

Skodsborg Strandvej 156  
DK-2942 Skodsborg  
Denmark

Patents ADP number (if you know it) 762839900 )

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4. Title of the invention

SPATIALLY DIRECTED INTERACTION ON A SOLID  
SURFACE

5. Name of your agent (if you have one)

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Spatially directed interaction on a solid surface

The present invention relates to methods for 5 performing interactions between a liquid or a component of the liquid and a solid surface, such as chemical reactions which may for instance be immobilisation or synthesis reactions on a solid surface, in which the location at which the interaction occurs is spatially defined by hydrodynamic 10 focusing or by electrodynamic focusing.

There is a requirement for being able to position or synthesise different chemical species in an array of row or spot locations on a micro-scale on the surface of a solid substrate. For instance, in conducting DNA hybridisation 15 studies there are proposals which require a "chip" having a surface on which every possible combination of a number of DNA bases is represented at a known and defined location, for instance every possible 8-mer.

Various screen printing techniques have been proposed 20 in the past for making such arrays. For instance US 5412087 is one example out of very many that describe methods of building such arrays by protecting a layer of chemical monomer sub-units put on a surface with a photo-labile protecting group, using a photo-mask to remove the protection 25 at selected locations by light exposure and reacting the next layer of chemical sub-units with the last layer at the unprotected locations. This process is repeated over and over to produce an array having a polymer synthesised on the surface and composed of different sequences of monomer units 30 (typically amino acids or nucleotide bases) at known row-column locations of the array.

It is known from "Biosensors and Bioelectronics Vol.13 No. 3-4, pages 427-438, 1998" that one can on a micro-scale choose the lateral position within a flow path occupied by the flow of a particular stream of liquid by altering the 5 proportion of a guide liquid which is introduced on either side of the stream of interest. This technique is termed 'hydrodynamic focussing'. The term 'hydrodynamic' is of course not to be understood as implying that the liquids employed must necessarily be wholly or in part aqueous. 10 Thus, it is disclosed there in relation to a flow switch that a flow of switchable liquid flowing in a covered trench 400  $\mu\text{m}$  wide and 50  $\mu\text{m}$  deep on the top of a silicon substrate can be guided to flow nearer either edge of the trench as desired. The flow is introduced through an inlet aligned 15 with the centre line of the trench. Two other inlets on either side of first inlet introduce a guide buffer flow. By choosing what proportion of the guide buffer flow comes in on each side without altering the total amount of guide buffer flow, the lateral position of the switchable flow within the 20 trench is varied. This determines through which of two outlets at the other end of the trench the hydrodynamically focused switchable flow exits.

Due to the small scale of the device, the Reynolds number of the flow is low and pure laminar flow is obtained. 25 There is therefore no mixing other than by diffusion between the guide buffer flows and the switchable flow.

Electrodynamic focusing (also known as electrokinetic focusing is described in US-A-5858187. It is disclosed that a flow of sample material across an intersection formed by a 30 sample channel and two focusing channels can be confined to

less than the width of the sample channel and that the focused flow can be laterally guided. Two modes of operation are disclosed. In one mode, there is a flow of sample liquid which is focused by two streams of focusing liquid produced 5 by electro-osmotic forces. In an alternative mode, the surface of the channel is coated to block the production of electro-osmotic force and liquid flow is prevented or is minimised. However, ionically charged materials in the sample are transported by electrophoretic force and follow 10 lines of electric potential which produce focusing of the sample material.

It is desirable to have available a wider range of 'wet chemistry' reaction techniques for immobilising reagents or reactants or carrying out chemical synthesis than are 15 consistent with the use of photo-labile protecting agents described above. Generally, conventional "wet chemistry" synthesis techniques offer inherently better yields than photo-chemical methods. Furthermore, such "wet chemistry" methods are better suited to providing in-process quality 20 control by measuring the reactants present on an on-going basis. Furthermore, there is a much more substantial knowledge base available, allowing better optimisation for specific uses and conditions. It is also desirable to have a 25 means of carrying out a wider range of site directed solid-liquid interactions such as magnetic or electrostatic capture interactions than is offered by the prior art.

The present invention now provides according to a first aspect a method for producing an interaction between a hydrodynamically focused liquid or a component of said

hydrodynamically focused liquid and a selected region of a target surface comprising:

5 providing said target surface as part of one of a plurality of surfaces together defining a flow path for liquid, the surface containing the target surface serving to define the width of the flow path,

10 providing for said flow path a set of three fluid inlets and at least one fluid outlet such that a flow of said hydrodynamically focused liquid can be directed into the flow path through one said inlet guided between two flows of guidance liquid introduced via the other two said inlets to leave said flow path through said at least one outlet,

15 providing for each pair of guidance liquid inlets flow control means such that the proportion of the total flow of guidance liquid introduced on each side of the said hydrodynamically focused liquid can be varied to position the flow of said hydrodynamically focused liquid laterally within the flow path, and

20 25 30 directing a flow of said hydrodynamically focused liquid and two flows of guidance liquid through respective ones of said inlets and along said flow path such that the flow of said liquid is directed over a selected region of said target surface having a width less than the width of the target surface and extending at a selected lateral position within said flow path controlled by selection of an appropriate flow ratio of guidance

liquid introduced on either side of the flow of said hydrodynamically focused liquid,

5 and allowing said hydrodynamically focused liquid or a component thereof to interact with said selected region of said target surface.

Said interaction between said hydrodynamically focused liquid and said target surface may involve a chemical 10 reaction. However, it should be appreciated that a wide range of forms of interaction are included. Thus, the interaction may be the capture of a species in the liquid by a magnetic field attracting said species to the surface. It may be the capture of a species in the liquid to the surface 15 by virtue of an inherent affinity, whether chemical or physical, between the surface and the substance. The term 'surface' in this context is not restricted to the upper boundary of the bulk substrate defining the flow channel but includes any material already present thereon. The affinity 20 may be due to the presence of one or more sources of magnetic attraction associated with the surface. Thus, one or more magnets may be used to attract paramagnetic beads out of a suspension in a liquid directed over a target region of the magnetically attractive surface. Similarly an electrically 25 charged surface may be used to attract and hold electrostatically or dielectrically attractable particles out of a liquid. Generally however, it will be understood that when the interaction in question is in the nature of a binding of the substance in question to the surface it will

be of a desired and generally specific nature and will not include a random or non-specific binding to the surface.

Where a chemical reaction is responsible for the interaction it may involve the formation of covalent or non-covalent bonds and may or may not involve the immobilisation of any substance to the surface as a result of the interaction. Thus, antibody/antigen specific binding interactions or oligonucleotide hybridisation reactions are contemplated as well as covalent synthesis reactions. 10 However, equally contemplated are chemical reactions in which a compound is stripped from a surface, such as the surface site specific dehybridisation of oligonucleotides or disruption of antibody/antigen complexes by chaotropic agents or the cleavage of a bound enzyme substrate by an enzyme in 15 the liquid. Also contemplated are reactions in which a component of the liquid reacts with the surface without binding, such as the reaction of an enzyme substrate in the liquid with an enzyme bound on the surface or vice versa.

It will be appreciated that the techniques described 20 herein are of enormously wide applicability and the above broad examples are merely a few of the types of interaction contemplated.

Where said interaction is a chemical reaction it may therefore be an immunoaffinity reaction, a nucleotide 25 hybridisation reaction, a chemical synthesis reaction, a chemical deprotection reaction, an enzyme catalysed reaction, or an enzyme inhibition reaction amongst other possibilities. Said reaction may comprise immobilising a first nucleotide or oligonucleotide on said surface. It may comprise covalently 30 adding a further nucleotide or oligonucleotide to a

nucleotide or oligonucleotide already immobilised on said surface.

Said reaction may comprise immobilising a first amino acid residue or a peptide on said surface. It may comprise 5 covalently adding a further amino acid or peptide to one already immobilised on said surface.

In order to preserve laminar flow of the guide and hydrodynamically focused flow streams the flow of liquid through said flow path is preferably at a Reynolds number of 10 no more than 10, but often it will be much less than this, for instance no more than 5, and generally no more than 1.

The linear flow rate through the flow channel may be quite high even at these low Reynolds numbers because of the small channel dimensions. Thus by way of example with a 15 channel 200  $\mu\text{m}$  wide and 40  $\mu\text{m}$  deep (cross sectional area 8000  $\mu\text{m}^2$ ) the volume flow rate might suitably be from 0.1 to 100  $\mu\text{l/min}$ . which corresponds to a linear flow rate of from 0.01 to 10  $\text{m/min}$ .

The flows of hydrodynamically focused liquid and of 20 guidance liquid may be produced by mechanical pumps, which preferably are electrically operated. However, the flow required for hydrodynamic focusing may alternatively be produced by electro-osmotic forces. If desired, the flow of one or more of the liquid streams may be produced by a pump 25 and the flow of one or more of the other liquid streams may be induced by electro-osmotic force.

The substrate in which said flow channel is formed may be made from any one of a large number of materials. Desirable properties are a high level of rigidity and the 30 ability to present an extremely smooth surface e.g. with

better than  $\pm 3 \mu\text{m}$ , preferably better than  $\pm 1 \mu\text{m}$ , most preferably no more than  $\pm 0.5 \mu\text{m}$  roughness. For many applications chemical inertness and an absence of non-specific binding for the hydrodynamically focused liquid or 5 its components will be desired. Generally the substrate should lend itself to the formation therein of a precisely dimensioned trench either by etching or an alternative process of material removal or by moulding. Suitable materials include glass, fused silica or silicon, in which 10 substrates the flow channel may be formed as a trench by etching.

An alternative preferred material is an engineering polymer such as polycarbonate, polypropylene, or polymethyl-methacrylate which can be precisely injection moulded to form 15 a shaped substrate providing such a trench for the flow channel. Such materials may be injection moulded using a nickel casting of an etched silicon master.

The surface of the substrate may be modified to increase its smoothness, to alter its hydrophobicity (e.g. by plasma 20 polymerisation of plastics) or its chemical inertness (e.g. by gold coating by vacuum deposition), if desired in selected locations.

Where electro-osmotic force is used to produce liquid flow, it will be necessary for the surface of the substrate 25 to be electrically charged when in contact with the liquid. For instance, silica is a suitable surface for this purpose as when in contact with an aqueous buffer liquid it will bear charged  $\text{Si-O}^-$  ions. Generally, materials useful in capillary electrophoresis will be suitable as substrates for use 30 according to this aspect of the invention.

A roof may then be provided over the trench to complete the flow channel, suitably by attaching a cover plate by adhesive. The cover plate may be of the same types of materials as are mentioned above but need not specifically be of the same material as the substrate containing the trench. The cover plate may be supported at a constant height across the width of the trench by pillar members.

Following the production of said interaction at said selected region of said target surface, a second interaction 10 may be conducted between a product of said first interaction and a second hydrodynamically focused liquid or component thereof at a selected sub-region forming part of said selected region by a method comprising:

providing a second plurality of surfaces together 15 defining a second flow path for liquid flow such that one of said surfaces intersects and has a portion in common with said target surface, the dimension of said one surface transverse to the direction of said second flow path defining the width of the second flow path,

20 providing for said second flow path a second set of three fluid inlets and at least one fluid outlet such that a flow of said second hydrodynamically focused liquid can be directed into the flow path through one said inlet guided between two flows of guidance liquid introduced via the other two said inlets to leave said flow path through said at least one outlet,

providing for each pair of guidance liquid inlets of the second flow path flow control means such that the proportion of the total flow of guidance liquid introduced on each side of the said second hydrodynamically focused liquid can be varied to position the flow of said second hydrodynamically focused liquid laterally within the second flow path, and

10 directing a flow of said second hydrodynamically focused liquid and two flows of guidance liquid through respective ones of said inlets and along said second flow path such that the flow of said liquid is directed over a selected sub-region of said common portion of 15 said target surface having a width less than the dimension of the common portion of the target surface in the width direction of the second flow path and lying at a selected lateral position within said second flow path controlled by selection of an appropriate flow ratio of 20 guidance liquid introduced on either side of the flow of said second hydrodynamically focused liquid,

25 and allowing said second hydrodynamically focused liquid or a component thereof to interact with the product of said first interaction on said selected sub-region of said target surface.

Thus according to a second aspect of the invention there is provided a method for producing an interaction between 30 hydrodynamically focused liquids or components of said

hydrodynamically focused liquids at a selected region of a target surface comprising:

5 providing said target surface at an intersection formed by two crossing flow paths defined by respective sets of flow path bounding surfaces,

10 each said set of bounding surfaces comprising a surface having a width that defines the width of its respective flow path, the target surface being defined by the intersection of said width defining surfaces,

15 providing for each flow path a set of three fluid inlets and at least one fluid outlet such that for each flow path, a flow of hydrodynamically focused liquid can be directed into the flow path through one said inlet guided between two flows of guidance liquid introduced via the other two said inlets to leave said flow path via said at least one outlet,

20 providing for each pair of guidance liquid inlets flow control means such that the proportion of the total flow of guidance liquid introduced on each side of the hydrodynamically focused liquid can be varied to position the flow of hydrodynamically focused liquid laterally within the respective flow path,

25 30 directing a flow of a first hydrodynamically focused liquid along one of said intersecting flow paths to carry out a first interaction between said first hydrodynamically focused liquid or a component thereof

and the target surface along a line extending at a selected lateral position within said flow path controlled by selection of an appropriate flow ratio of guidance liquid introduced on either side of the flow of hydrodynamically focused liquid, said interaction producing a product on said target surface,

5 stopping flow through said one flow path,

10 directing a flow of a second hydrodynamically focused liquid along the other one of said intersecting flow paths to carry out a second interaction between said second hydrodynamically focused liquid or a component thereof and the product of said first interaction on said target surface at a point within the intersection of the flow paths lying along a line extending at a selected lateral position within said other flow path controlled by selection of an appropriate flow ratio of guidance liquid introduced on either side of the flow of 15 said second hydrodynamically focused liquid,

20

whereby said second interaction takes place at a selected location within the area of intersection of the two flow paths defined by the selected lateral positions 25 of said hydrodynamically focused liquid flows.

The invention includes apparatus for use in accordance with the second aspect of the invention by producing an interaction between hydrodynamically focused liquids or

components of said hydrodynamically focused liquids at a selected region of a target surface comprising:

5 a substrate defining said target surface at an intersection formed by two crossing flow paths defined by respective sets of flow path bounding surfaces of the substrate,

10 each said set of bounding surfaces comprising a surface having a width that defines the width of its respective flow path, the target surface being defined by the intersection of said width defining surfaces,

15 a set of three fluid inlets and at least one fluid outlet associated with each said flow path such that for each flow path, a flow of hydrodynamically focused liquid can be directed into the flow path through one said inlet guided between two flows of guidance liquid introduced via the other two said inlets to leave said flow path via said at least one outlet, and

20 flow control means associated with each pair of guidance liquid inlets such that the proportion of the total flow of guidance liquid introduced on each side of the respective hydrodynamically focused liquid can be varied to position the flow of hydrodynamically focused liquid laterally within the respective flow path.

The apparatus may further comprise means for producing said flow of hydrodynamically focused liquid and means for producing said flows of guidance liquid. Said means may 5 comprise a respective pump for each flow. Said flow control means may then be constituted by means for controlling the rate at which each pump operates or by means for controlling the resistance to flow against which each pump works.

Alternatively, the means for producing the required flow 10 may be electrodes provided upstream and downstream of said intersection in the flow path for the hydrodynamically focused liquid and in the flow path of each guidance liquid and the means for controlling the flow may then be constituted by means for adjusting the respective voltages 15 applied to the electrodes.

Such apparatus preferably further comprises a detector for detecting and/or quantitating at selected locations of said target surface products or results of the interactions of said hydrodynamically focused liquids.

20 The nature of the detector required will vary according to the nature of the interactions to be monitored but the detector may by way of example be a fluorescence detector, a radioactivity detector, a microscope, a confocal microscope, a luminescence detector, a spectrophotometer, or a photo-luminescence detector. An appropriately responsive 25 photographic film, e.g. an X-ray film, may be used on the detector.

Where the product of the method of the invention is an oligonucleotide array, electrodes may be provided below the 30 substrate surface or at the substrate surface in order to

enable the user of the array to carry out electrically promoted hybridisation or denaturation, as known in the art.

According to a third aspect of the invention, there is provide a method for producing an interaction between a 5 component of a liquid and a selected region of a target surface, comprising providing a said target surface in contact with a medium through which charged molecules can be caused to migrate, providing oppositely charged driving electrodes at opposed locations of said target surface in 10 electrical contact with said medium to define a migration path between said driving electrodes, providing guiding electrodes of like charge on opposed sides of said migration path in electrical contact with said medium, supplying charged molecules to a starting location in said medium in 15 said migration path and causing said molecules to migrate in said migration path away from one said driving electrode and towards the other said driving electrode whilst laterally electrodynamically focusing said migrating charged molecules to confine their movement within substantially less than the 20 whole width of said migration path by the application of controlled voltages to said guiding electrodes so that the molecules migrate over said selected region of said target surface, and allowing said electrodynamically focused molecules to interact with said target surface. Such a 25 method provides focusing by the use of electrophoretic force rather than by hydrodynamic focusing. The method may readily be adapted to provide electrodynamically focused migration first in one direction and subsequently in a second direction crosswise of the first direction in a similar manner to that 30 in which hydrodynamic focusing is used according to the

second aspect of the invention. Interactions may be carried out and monitored generally as described above in the context of the first and second aspects of the invention.

The invention will be further described and illustrated 5 by the following description of preferred embodiments with reference to the accompanying drawings, in which:

Figure 1 shows in plan view an example of apparatus in use in a method according to the first aspect of the invention;

10 Figure 2 shows in plan view apparatus according to the invention suited for use in accordance with the second aspect of the invention;

15 Figure 3 shows in plan view a detail of the apparatus of Figure 2 in use in a method in accordance with the second aspect of the invention;

Figure 4 shows schematically a section on the line IV-IV in Figure 2;

Figure 5 shows in plan view an alternative apparatus for use in accordance with the first aspect of the invention; and

20 Figure 6 shows in plan view apparatus for use in accordance with the third aspect of the invention.

As shown in Figure 1, apparatus for use in accordance with the method of the first aspect of the invention comprises a substrate 10. This is preferably chosen to be a material of high dimensional stability capable of being formed with a flow channel 12 of precisely defined and stable dimensions. The flow channel 12 takes the form of a trench having a floor 14 and side walls 16. A roof 18 (as in Figure 4) is provided over the trench by a plate suitably of the 30 same material cemented over the trench.

The flow channel defines a flow path which extends left to right in the drawing and has at its upstream end three inlets for liquid. The centre inlet 20 is for a flow of hydrodynamically focused liquid 26. Each of the inlets 22 5 and 24 is for a respective flow of guidance liquid 28. The end of the flow path provided with an outlet for the liquids at 30. Each of the inlets and the outlet has a respective flow control valve 32, 34, 36, 38 (as in Figure 2).

The dimensions of the flow channel may be chosen within 10 wide limits according to the nature of the interaction it is desired to carry out. The main limiting factor will generally be the need to maintain substantially pure laminar flow so that the hydrodynamically focused liquid and the guidance liquids do not mix. Generally, provided the height 15 of the flow channel is sufficiently small, say 40  $\mu\text{m}$ , the width may be up to 10mm or more. Pillars may be provided extending between the floor and the roof of the flow channel to maintain the appropriate height spacing.

Generally, for a rectangular section channel, the 20 appropriate length to height to width relationship is chosen to maintain laminar flow at the chosen flowrate, according to known formulae.

The methods described herein are operable over wide ranges of temperature, compatible with the liquids used 25 remaining liquid.

Liquids are suitably driven through the apparatus by the use of syringe pumps or similar, suitably driven by stepper motors.

Care should generally be taken to avoid the formation of 30 bubbles in all of the liquids used.

By way of example, there follows a description of the use of the apparatus so far described in making one dimensional and two dimensional oligonucleotide arrays, but the same principles may be readily adapted for making similar 5 arrays of a different chemical nature, e.g. peptide arrays.

As the chemical techniques appropriate to synthesising oligonucleotides on a solid substrate are well known in the art no detailed account will be given here and the relevant principle will be explained with reference to a simplified 10 account of the relevant chemical steps. Details of suitable methods to be adapted for use according to the invention are for instance to be found in Carruthers M.H., Beaton, G., Wu J.V. and Wisher W., Methods in Enzymology (1992) 211:3-20. The surface of the floor of the flow channel is first made 15 ready to react with a first nucleotide base in a known manner. A solution of a first desired base in a suitably reactive form (let us say adenine (A)) is introduced as flow 20 of hydrodynamically focused liquid and two flows of guidance buffer are introduced through inlets 22 and 24. The 25 proportions of the total flow of guidance buffer introduced through these respective inlets are chosen so that the flow 26 is deflected laterally (vertically in the drawing) to the desired extent and in the desired direction from the centre line so that the hydrodynamically focused flow proceeds down a line within the flow channel and reaction of the base A with the surface is restricted to that line. The adenine solution may then be replaced with buffer so as to flush the adenine solution from the system and further reagents may be sent down the same line to carry out any deprotection or

protection reactions required by the general reaction scheme at this stage.

Following this, the relative flows of guidance buffer may be readjusted whilst keeping the total flow rate of 5 guidance buffer constant so as to redirect the flow 26 downwardly to the next desired level and a second nucleotide (let us say guanine (G)) may be reacted with the surface along a line at that level. The width of each line may be extremely small e.g. from 1 to 180  $\mu$ m.

10 Similar parallel tracks of the bases cytosine (C) and thymine (T) may be laid down in similar fashion and the sequence may be repeated as often as desired, thus providing a first layer of bound nucleotides in a one dimensional array.

15 Going back to the first track laid down (which was of base A) one can then lay down a track of a second base chosen from any one of A, T, C and G carrying out all necessary rinsing, protection and deprotection steps in accordance with the reaction scheme as one proceeds.

20 The process may be repeated as often as desired to produce a one dimensional oligonucleotide array in which each row contains a known oligonucleotide sequence.

25 By combining the processes described above with known photo-masking and photo-deprotection reactions a two dimensional array may be created.

Thus once the initial layer has been completed as previously described, a specific line of spots along the first track of base A laid down may be deprotected by a light activated photo-deprotection reaction. The next base 30 introduced along that same line will then react only at the

deprotected spots. A second base may then be reacted at a different set of spots deprotected along the same line through a different mask and so on such that along the first line laid down there are now numerous spots with each of the 5 possible combinations AA, AT, AC, and AG.

This may then be repeated for each of the subsequent lines and over many layers to build a two dimensional array in which at each row/column intersection there is an oligonucleotide of a unique and known sequence.

10 The apparatus shown in Figures 2 to 4 lends itself to the building up of a two dimensional array of oligonucleotides or other polymers having a similar defined sequence of differing monomer subunits by a significantly different process in accordance with the second aspect of the 15 invention.

The apparatus of Figure 2 resembles that shown in Figure 1 except in the following manner. A second flow channel 40 is defined like flow channel 12 by a trench in the substrate 10 having a floor 42 (Figs. 3 and 4) and side walls 44 (Fig. 20 3). The roof 18 is again provided and of course covers both flow channels.

The flow channel 40 defines a flow path which extends from the bottom to the top in the drawing and has at its upstream end three inlets for liquid. The centre inlet 48 is 25 for a flow of hydrodynamically focused liquid 60. Each of the inlets 50 and 52 is for a respective flow of guidance liquid 62. The end of the flow path is provided with an outlet for the liquids at 54. Each of the inlets and the outlet has a respective flow control valve 66, 68, 70 and 72.

The flow channels 12 and 40 preferably, but not essentially, cross at right angles as shown and at their intersection, the floors of the flow channels share a region of the substrate 10 in common at 74 (Fig. 3) constituting a 5 target surface. Preferably, the corners formed in the side walls of the flow channels at their intersection are radiused rather than hard.

Extending the previous account of building a one dimensional oligonucleotide array by way of example, after 10 the first layer of lines of single nucleotide bases has been laid down as described with reference to Figure 1 (all conducted with inlets 48-52 and outlet 64 closed, one may then shut the inlet valves 32-34 and outlet valve 38 and pass a flow of a hydrodynamically focused liquid 60 containing a 15 selected nucleotide base through the flow channel 40 at a left-right position selected by the proportion of buffer liquid passed through each of the inlets 50,52. Subsequent lines of different bases may be laid down in selected positions such that at each row column intersection 76 (Fig. 20 3) one has a defined di-nucleotide sequence.

Further layers of rows may then be laid down alternately in the flow channels 12 and 40 to build oligonucleotides of any desired length with each row-column position containing a known oligonucleotide sequence.

25 By way of example, all possible 8-mers of oligonucleotides may be formed by putting down in a first layer 64 rows of A, followed by 64 rows of T, then 64 rows of C and 64 rows of G. Next one lays down 64 columns of each of A,T,C and G. Then one lays down four repeating sequences of 16 30 rows of each of A,T,C, and G and then four repeating

sequences of 16 columns of A,T,C and G. This is followed by  
16 repeating sequences of 4 rows of each base and then  
by sixteen repeating sequences of 4 columns of each base.  
Lastly one lays down 256 single rows and then 256 single  
5 columns of each base in order. Each layer of rows or columns  
covers the entire area with 256 rows or columns in each  
layer.

If each row and column is made about 3  $\mu\text{m}$  wide, one has  
patches of approximately  $10 \mu\text{m}^2$  arranged in an orthogonal 2-  
10 dimensional array, each containing a single unique 8-mer  
sequence at a known position within the array.

Where a number of adjacent rows of the same base are to  
be laid down, they need not be done individually. The  
hydrofocussed flow may be made broader to cover the desired  
15 area in one pass by adjusting the amounts of guide buffer and  
hydrodynamically focussed flow liquid.

If desired, more than one substrate 10 may be connected  
simultaneously to the control valves 32-38. There may be a  
stack of several substrates connected to said valves via  
20 suitable manifolds so that the operations described above can  
be carried out on all the substrates in the stack  
simultaneously. This is a particularly useful arrangement  
for producing numbers of identical substrates bearing lines  
or spots of molecules laid down on synthesised on the  
25 substrate.

As indicated in Figure 4, the apparatus may include a  
detector 80 for detecting and/or quantitating an interaction  
produced on the surface. For instance, the 8-mer array just  
described may be exposed to a labelled oligonucleotide of  
30 unknown sequence and the point in the array where

hybridisation occurs may be determined using a suitable detector. The nature of the detector desired will vary widely according to the nature of the substances interacting on the surface and labelling methods used.

5 As shown in Figure 5, apparatus similar to that of Figure 1 may be driven by electro-osmotic force. Each inlet 20, 22, 24 and the outlet 30 is provided with a respective electrode 520, 522, 524 and 530. Suitably each electrode may be situated in contact with a reservoir from which the 10 respective liquid is supplied or (in the case of the outlet 30) to which the liquid is directed. The surface of the substrate bears an ionic charge as described above. This attracts a boundary layer of oppositely charged solvated ions in the liquid which are drawn by electrophoretic force toward 15 the outlet electrode 530. Because the ions are solvated, this produces a flow of liquid. The flow rate from each inlet may be adjusted by control of the potential difference between its respective electrode and the outlet electrode 530. Typical operating voltages are from 1-10 kV. Due to 20 the high resistance posed by the very small cross section of the flow channels, such high voltages may be used without producing excessive current and hence without excessive heat production.

The lateral position of the hydrodynamically focused flow is controlled by balancing the voltages applied to the 25 guidance flow electrodes 522 and 524.

A similar modification may be applied to the apparatus of Figure 3.

If the surface of the substrate is such that electro- 30 osmotic flow is not generated (or not to a significant

extent), the apparatus shown in Figure 5 can nonetheless be operated according to the third aspect of the invention. Thus, if the surface of the substrate is not ionic, e.g. is coated with polyacrylamide, electro-osmotic flow will not 5 occur and there will be no hydrodynamic focusing. However, charged molecules such as proteins or nucleic acids will migrate by electrophoretic forces from the inlet 20 towards the outlet 30 and will follow a focused laterally restricted track between the inlets 22 and 24 following the electric 10 field vectors defined by the electrodes.

However, operating in this mode, there is no necessity to provide the guidance liquid on either side as shown in Figure 5. Instead, as shown in Figure 6, one may have a substrate 60 defining a target surface over which is a 15 stationary liquid or gel medium. A pair of driving electrodes 62, 64 are positioned at opposite ends of the target surface, in electrical content with the medium. A migration path is thereby defined between the electrodes 62, 64. Although only one electrode 62 and one electrode 64 is 20 shown, if desired a row of separate electrodes 62 or of electrodes 64 (or both) may be provided. On opposite lateral sides of the migration path between the electrodes 62, 64 are provided guidance electrodes 66, 68. Again, if desired a row 25 of separate electrodes may be provided instead of the single elongate electrode shown.

Controlled electrical voltages are applied to the driving and guidance electrodes via a suitable controlled voltage source. As shown, the voltage applied to one of the driving electrodes is opposite in sign to that applied to the 30 other three electrodes. Negatively charged molecules

introduced at the driving electrode 62 will migrate in the medium towards the electrode 64 and will be laterally spatially confined or focused by the guidance electrodes 66, 68. The migration can be directed closer or further from the 5 electrode 66 by suitable adjustment of the voltages applied to the two guidance electrodes 66, 68. The target surface defined between the electrodes may be similar in size to the target surface in the apparatus of Figures 1 to 4. Suitable voltages to drive the electrodynamically focused migration 10 between the driving electrodes may be in the range of 0.5 to 10 kV/cm, e.g. 1-5 kV/cm. Whereas in the case of hydrodynamic focusing the channel dimensions are limited by the need to maintain laminar flow, in the case of purely electrophoretic driven electrodynamic focusing, the limiting 15 factor may be the need to restrict heat generation.

The sign of the voltage applied to the electrodes in Figures 5 and 6 need not be as shown but may be chosen with regard to the nature of the substrate and the charge of the molecules to be focused.

20 After migration of molecules from electrode 62 to electrode 64 and interaction with the target surface, electrodes 66 and 68 may be used as driving electrodes and electrodes 62 and 64 may be used as guidance electrodes, with suitable reconfiguration of the applied voltages, so as to 25 migrate molecules from electrode 66 to electrode 68, i.e. crosswise of the initially described migration.

Thus by way of further example, the surface may be 30 coated uniformly with a first reactant, for instance an antibody, and a sample with a concentration of a binding partner for the antibody that varies over time may be

progressively scanned over the surface using the apparatus of Figure 1 so that each row represents interaction between the flow and the surface over a defined time period. The concentration of the binding partner during each time period 5 may then be determined by measuring the amount of binding in each row. As a variation of this, columns of different antibodies may be provided using the apparatus of Figure 2 and the sample may then be scanned down the surface as previously described so that each row now gives a measurement 10 of the amount of each respective antibody binding partner present in the sample during each time period.

In a further example of the use of the invention, the array of locations definable according to the practice of the invention may be used in a microscopic version of a conventional microtitre plate. Thus, virtual wells 15 constituted by points in the array may be coated with an antibody or antigen (the whole surface of the substrate within the flow channel may be so coated) and the method described with respect to figure 1 may be used to expose 20 respective rows of locations to a sample and to various concentrations of standard sequentially, followed by other conventional assay reagents with the resulting reaction product concentrations being read by the detector so that each row provides a number of 'repeats' corresponding to 25 column locations within the row and the different rows provide calibration curve information as well as the result for the sample. Many variations on this theme will readily occur to those skilled in the art.

Generally the invention will have utility in clinical 30 diagnostics, environmental monitoring, quality control, food

technology and pharmaceutical screening, including use in toxicity studies, genomics and proteomics. Sample materials that may be studied using apparatus and methods according to the invention will include body fluids, nucleotide based 5 materials including DNA and RNA, proteins, peptides, polypeptides, cell culture products, waste water, drinking water and ground water. The methods and apparatus described will have wide application in combinatorial chemistry.

Very many other modifications and variations of the 10 invention as described above in its various exemplified embodiments will also readily occur to those skilled in the art.

## Claims:

1. A method for producing an interaction between a hydrodynamically focused liquid or a component of said 5 hydrodynamically focused liquid and a selected region of a target surface comprising:

providing said target surface as part of one of a plurality of surfaces together defining a flow path for 10 liquid flow, the dimension of the surface containing the target surface transverse to the direction of said flow path serving to define the width of the flow path,

providing for said flow path a set of three fluid inlets 15 and at least one fluid outlet such that a flow of said hydrodynamically focused liquid can be directed into the flow path through one said inlet guided between two flows of guidance liquid introduced via the other two said inlets to leave said flow path through said at 20 least one outlet,

providing for each pair of guidance liquid inlets flow 25 control means such that the proportion of the total flow of guidance liquid introduced on each side of the said hydrodynamically focused liquid can be varied to position the flow of said hydrodynamically focused liquid laterally within the flow path and at a desired lateral position over the target surface, and

directing a flow of said hydrodynamically focused liquid and two flows of guidance liquid through respective ones of said inlets and along said flow path such that the flow of said liquid is directed over a selected region of said target surface having a width less than the width of the target surface and extending at a selected lateral position within said flow path controlled by selection of an appropriate flow ratio of guidance liquid introduced on either side of the flow of said hydrodynamically focused liquid,

and allowing said hydrodynamically focused liquid or a component thereof to interact with said selected region of said target surface.

2. A method as claimed in Claim 1, wherein said interaction between said hydrodynamically focused liquid and said target surface involves a chemical reaction.
3. A method as claimed in Claim 2, wherein said chemical reaction is an immunaffinity reaction, a nucleotide hybridisation reaction, a chemical synthesis reaction, a chemical deprotection reaction, an enzyme catalysed reaction, an enzyme inhibition reaction.
4. A method as claimed in Claim 2, wherein said reaction comprises immobilising a first nucleotide or oligonucleotide on said surface.

5. A method as claimed in Claim 3, wherein said reaction comprises covalently adding a further nucleotide or oligonucleotide to a nucleotide or oligonucleotide already immobilised on said surface.
6. A method as claimed in Claim 2, wherein said reaction comprises immobilising a first amino acid residue or a peptide on said surface.
- 10 7. A method as claimed in Claim 3, wherein said reaction comprises covalently adding a further amino acid or peptide to one already immobilised on said surface.
- 15 8. A method as claimed in any preceding claim, wherein the flow of liquid through said flow path is at a Reynolds number of no more than 10.
- 16 9. A method as claimed in Claim 8, wherein the flow of liquid through said flow path is at a Reynolds number of no more than 5.
- 20 10. A method as claimed in Claim 8, wherein the flow of liquid through said flow path is at a Reynolds number of no more than 1.
- 25 11. A method as claimed in any preceding claim, wherein said flow channel is produced by etching of a glass, fused silica or silicon substrate.

12. A method as claimed in any one of claims 1 to 10, wherein said flow channel is produced by injection moulding of plastics to form a shaped substrate.

5 13. A method as claimed in any preceding claim, wherein following the production of said interaction at said selected region of said target surface, a second interaction is conducted between a product of said first interaction and a second hydrodynamically focused liquid or component thereof at a selected sub-region forming 10 part of said selected region by a method comprising:

15 providing a second plurality of surfaces together defining a second flow path for liquid flow such that one of said surfaces intersects and has a portion in common with said target surface, the dimension of said one surface transverse to the direction of said second flow path defining the width of the second flow path,

20 providing for said second flow path a second set of three fluid inlets and at least one fluid outlet such that a flow of said second hydrodynamically focused liquid can be directed into the flow path through one said inlet guided between two flows of guidance liquid introduced via the other two said inlets to leave said 25 flow path through said at least one outlet,

30 providing for each pair of guidance liquid inlets of the second flow path flow control means such that the proportion of the total flow of guidance liquid

introduced on each side of the said second hydrodynamically focused liquid can be varied to position the flow of said second hydrodynamically focused liquid laterally within the second flow path,

5 and

10 directing a flow of said second hydrodynamically focused liquid and two flows of guidance liquid through respective ones of said inlets and along said second flow path such that the flow of said liquid is directed over a selected sub-region of said common portion of said target surface having a width less than the width of the second flow path and lying at a selected lateral position within said second flow path controlled by 15 selection of an appropriate flow ratio of guidance liquid introduced on either side of the flow of said second hydrodynamically focused liquid,

20 and allowing said second hydrodynamically focused liquid or a component thereof to interact with the product of said first interaction on said selected sub-region of said target surface.

25 14. A method for producing an interaction between hydrodynamically focused liquids or components of said hydrodynamically focused liquids at a selected region of a target surface comprising:

providing said target surface at an intersection formed by two crossing flow paths defined by respective sets of flow path bounding surfaces,

5 each said set of bounding surfaces comprising a surface having a width that defines the width of its respective flow path, the target surface being defined by the intersection of said width defining surfaces,

10 providing for each flow path a set of three fluid inlets and at least one fluid outlet such that for each flow path, a flow of hydrodynamically focused liquid can be directed into the flow path through one said inlet guided between two flows of guidance liquid introduced 15 via the other two said inlets to leave said flow path via said at least one outlet,

20 providing for each pair of guidance liquid inlets flow control means such that the proportion of the total flow of guidance liquid introduced on each side of the hydrodynamically focused liquid can be varied to position the flow of hydrodynamically focused liquid laterally within the respective flow path,

25 directing a flow of a first hydrodynamically focused liquid along one of said intersecting flow paths to carry out a first interaction between said first hydrodynamically focused liquid or a component thereof and the target surface along a line extending at a 30 selected lateral position within said flow path

controlled by selection of an appropriate flow ratio of guidance liquid introduced on either side of the flow of hydrodynamically focused liquid, said interaction producing a product on said target surface,

5

stopping flow through said one flow path,

10 directing a flow of a second hydrodynamically focused liquid along the other one of said intersecting flow paths to carry out a second interaction between said second hydrodynamically focused liquid or a component thereof and the product of said first interaction on said target surface at a point within the intersection of the flow paths lying along a line extending at a 15 selected lateral position within said other flow path controlled by selection of an appropriate flow ratio of guidance liquid introduced on either side of the flow of said second hydrodynamically focused liquid,

20

whereby said second interaction takes place at a selected location within the area of intersection of the two flow paths defined by the selected lateral positions of said hydrodynamically focused liquid flows.

25 15. A method as claimed in any preceding claim, wherein said flow of hydrodynamically focused liquid and said flows of guidance liquid are electro-osmotic flows.

16. Apparatus for use in producing an interaction between 30 hydrodynamically focused liquids or components of said

hydrodynamically focused liquids at a selected region of a target surface comprising:

5 a substrate defining said target surface at an intersection formed by two crossing flow paths defined by respective sets of flow path bounding surfaces of the substrate,

10 each said set of bounding surfaces comprising a surface having a width that defines the width of its respective flow path, the target surface being defined by the intersection of said width defining surfaces,

15 a set of three fluid inlets and at least one fluid outlet associated with each said flow path such that for each flow path, a flow of hydrodynamically focused liquid can be directed into the flow path through one said inlet guided between two flows of guidance liquid introduced via the other two said inlets to leave said flow path via said at least one outlet, and

20 25 flow control means associated with each pair of guidance liquid inlets such that the proportion of the total flow of guidance liquid introduced on each side of the respective hydrodynamically focused liquid can be varied to position the flow of hydrodynamically focused liquid laterally within the respective flow path.

17. Apparatus as claimed in Claim 16, further comprising a detector for detecting and/or quantitating at selected locations of said target surface products of the interactions of said hydrodynamically focused liquids.

5

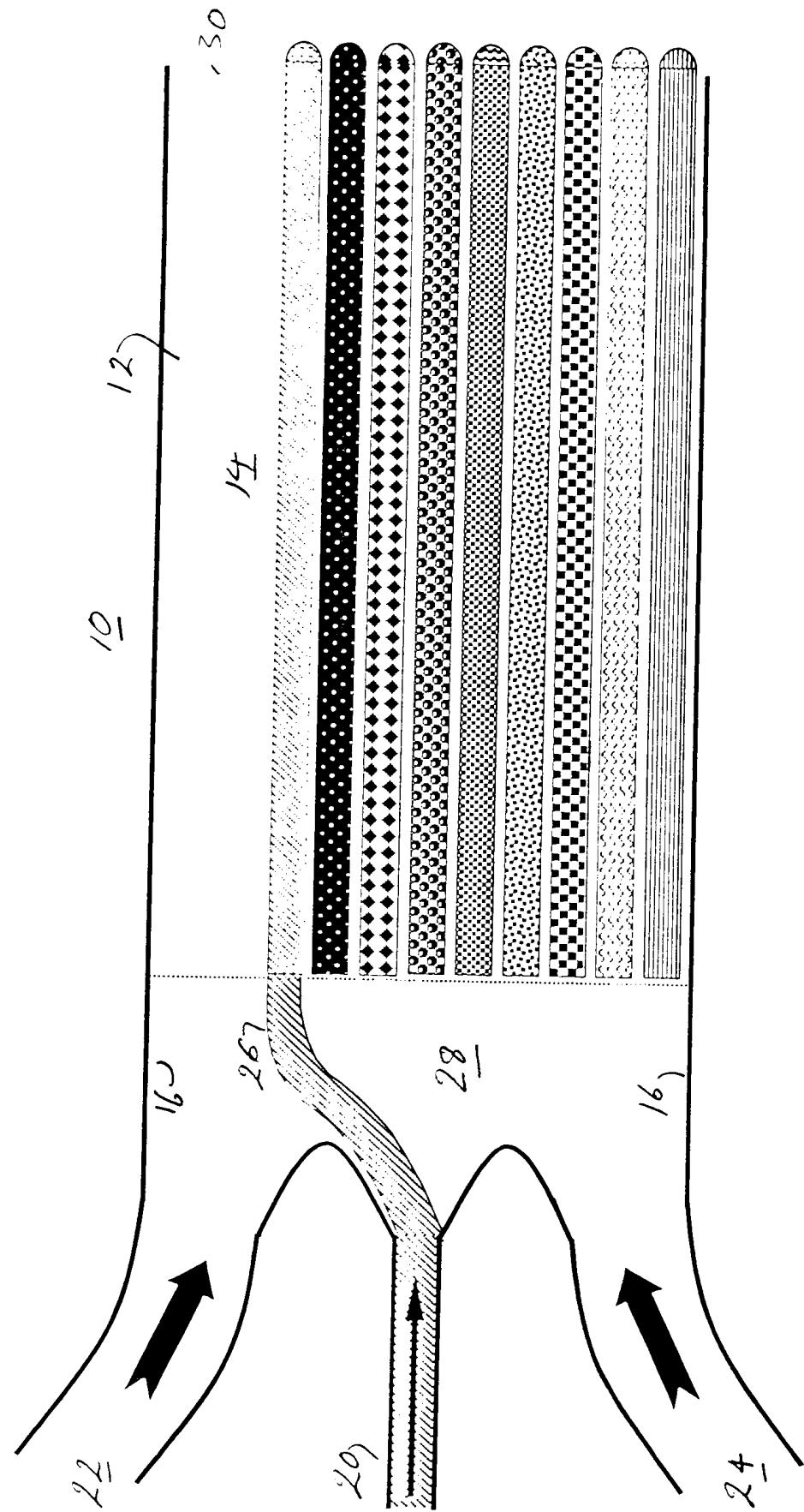
18. A method for producing an interaction between a component of a liquid and a selected region of a target surface, comprising providing a said target surface in contact with a medium through which charged molecules can be caused to migrate, providing oppositely charged driving electrodes at opposed locations of said target surface in electrical contact with said medium to define a migration path between said driving electrodes, providing guiding electrodes of like charge on opposed sides of said migration path in electrical contact with said medium, supplying charged molecules to a starting location in said medium in said migration path and causing said molecules to migrate in said migration path away from one said driving electrode and towards the other said driving electrode whilst laterally electro-dynamically focusing said migrating charged molecules to confine their movement within substantially less than the whole width of said migration path by the application of controlled voltages to said guiding electrodes so that the molecules migrate over said selected region of said target surface, and allowing said electro-dynamically focused molecules to interact with said target surface.

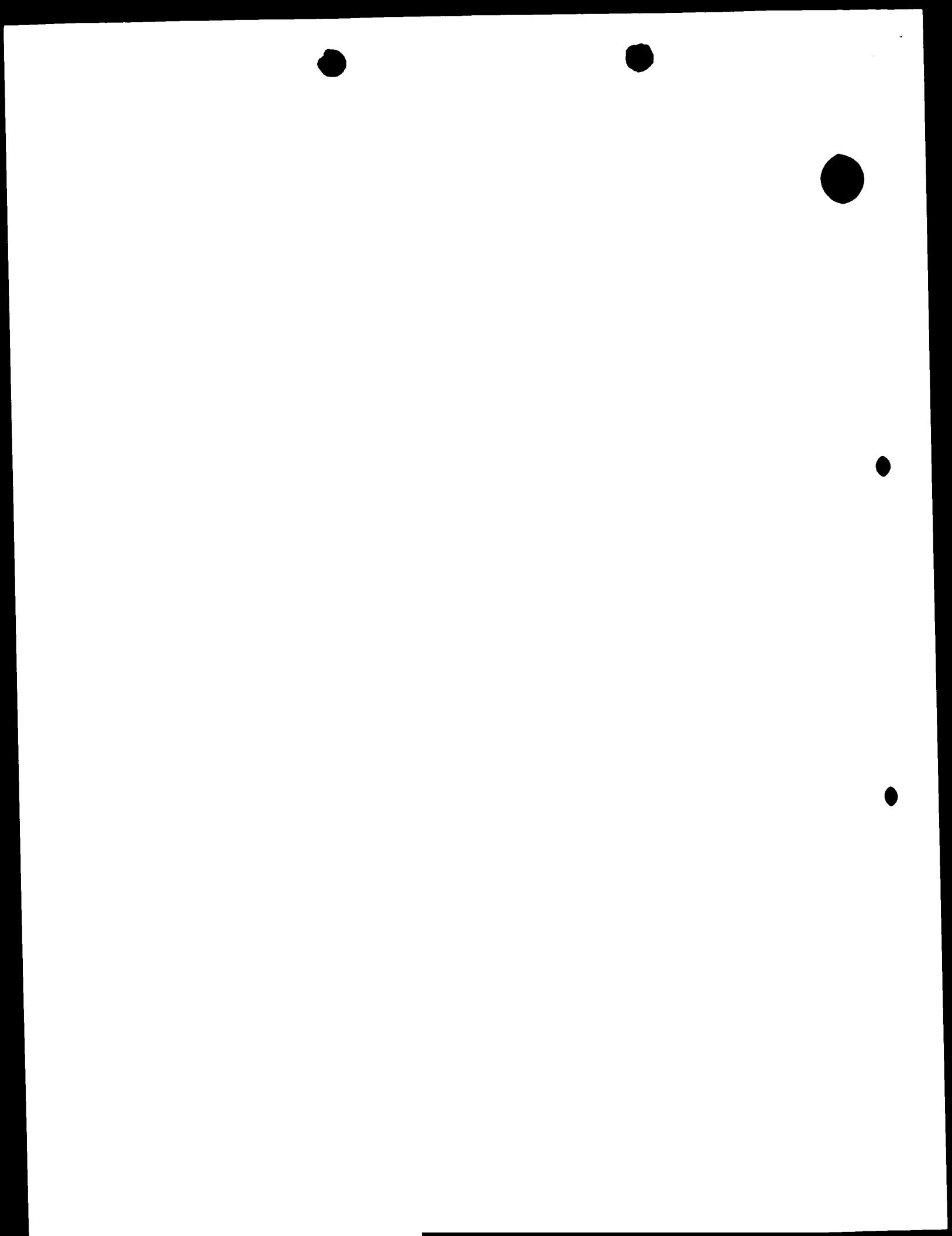
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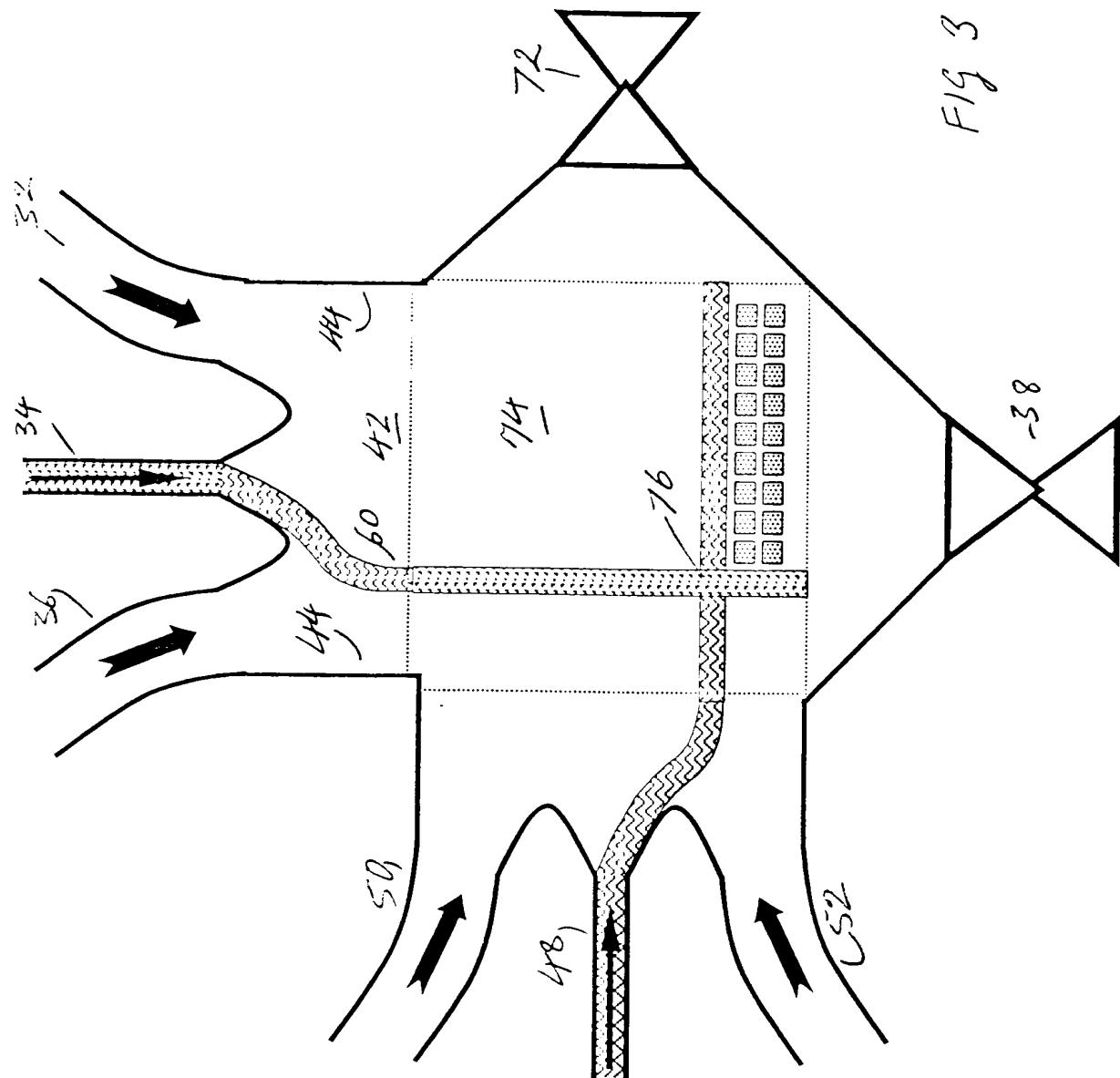
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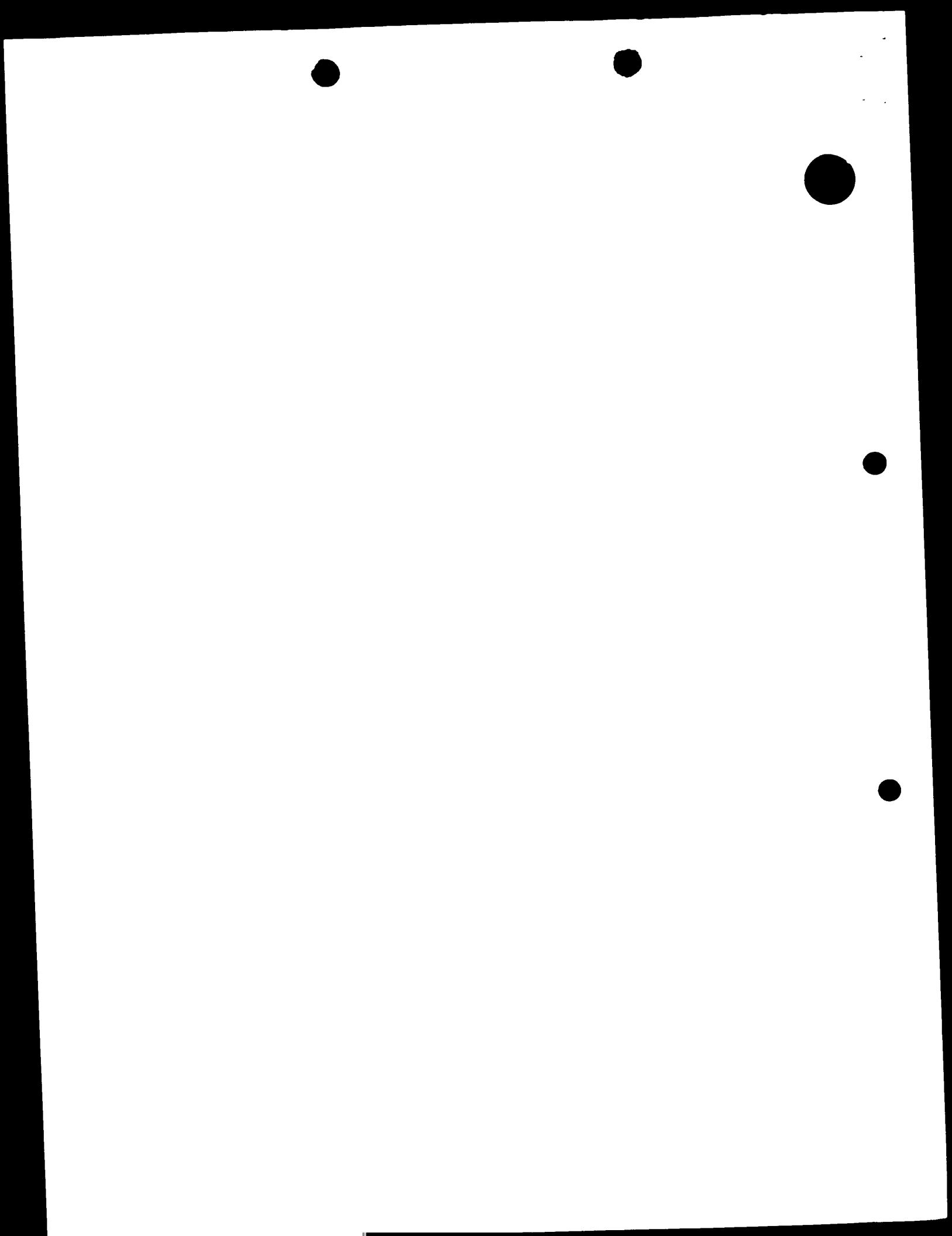




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Fig 3





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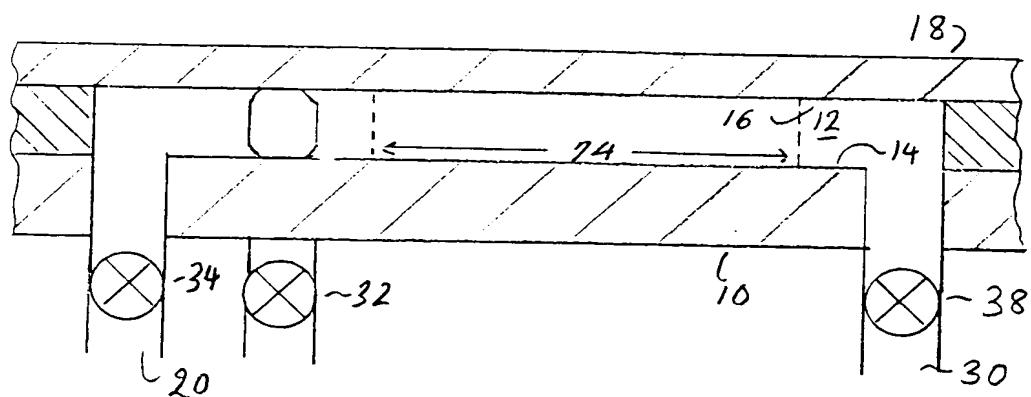
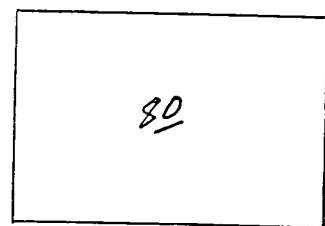
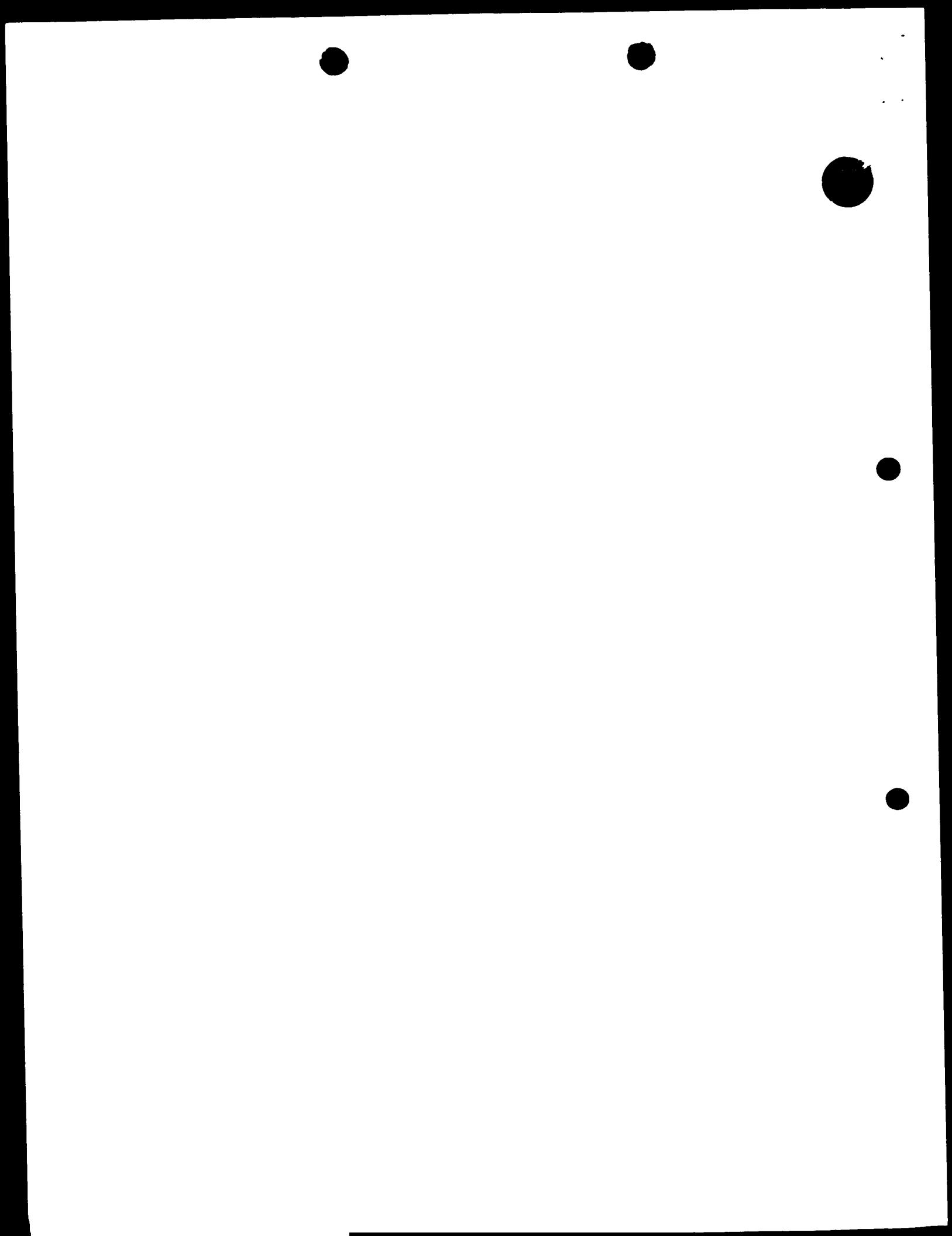
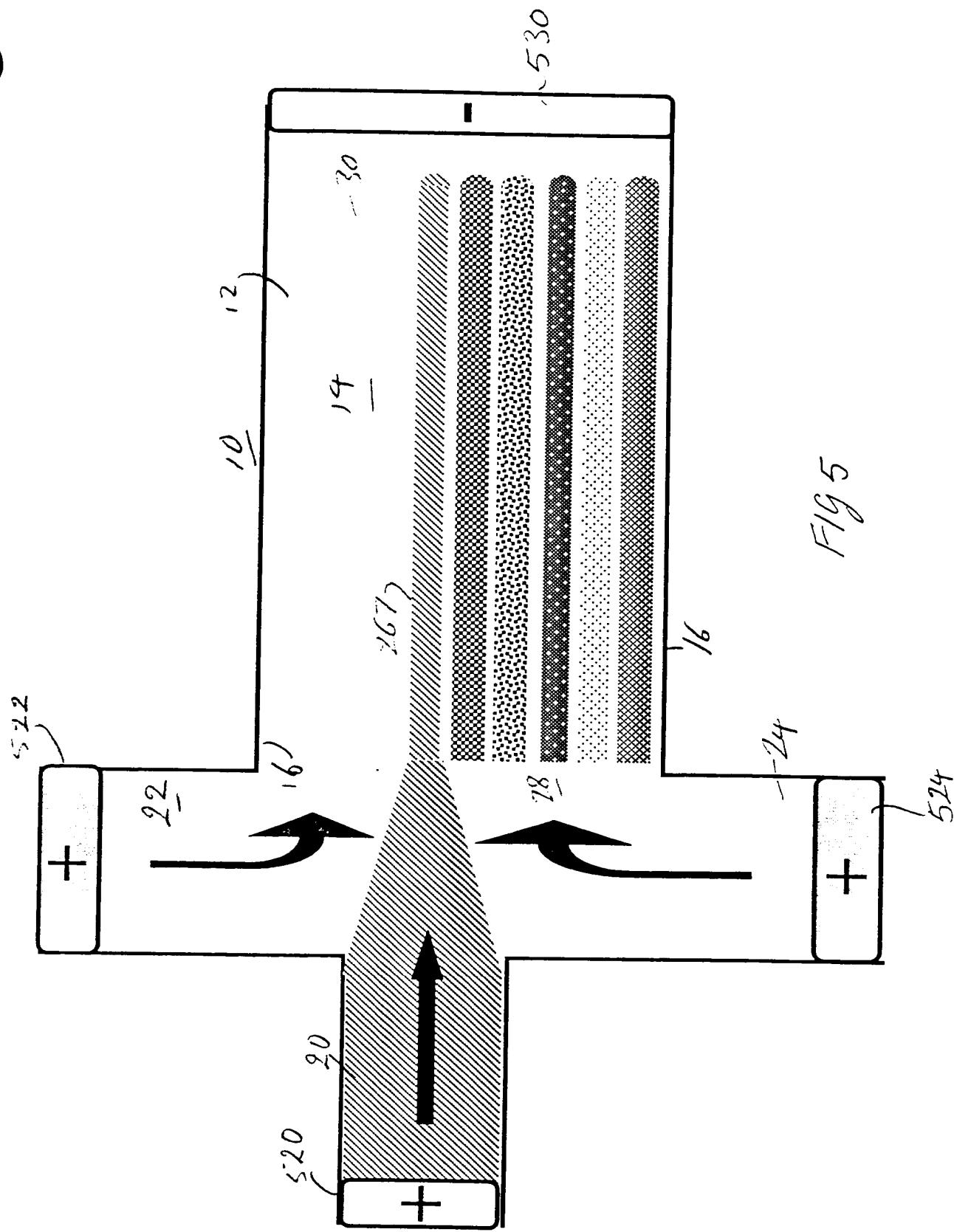
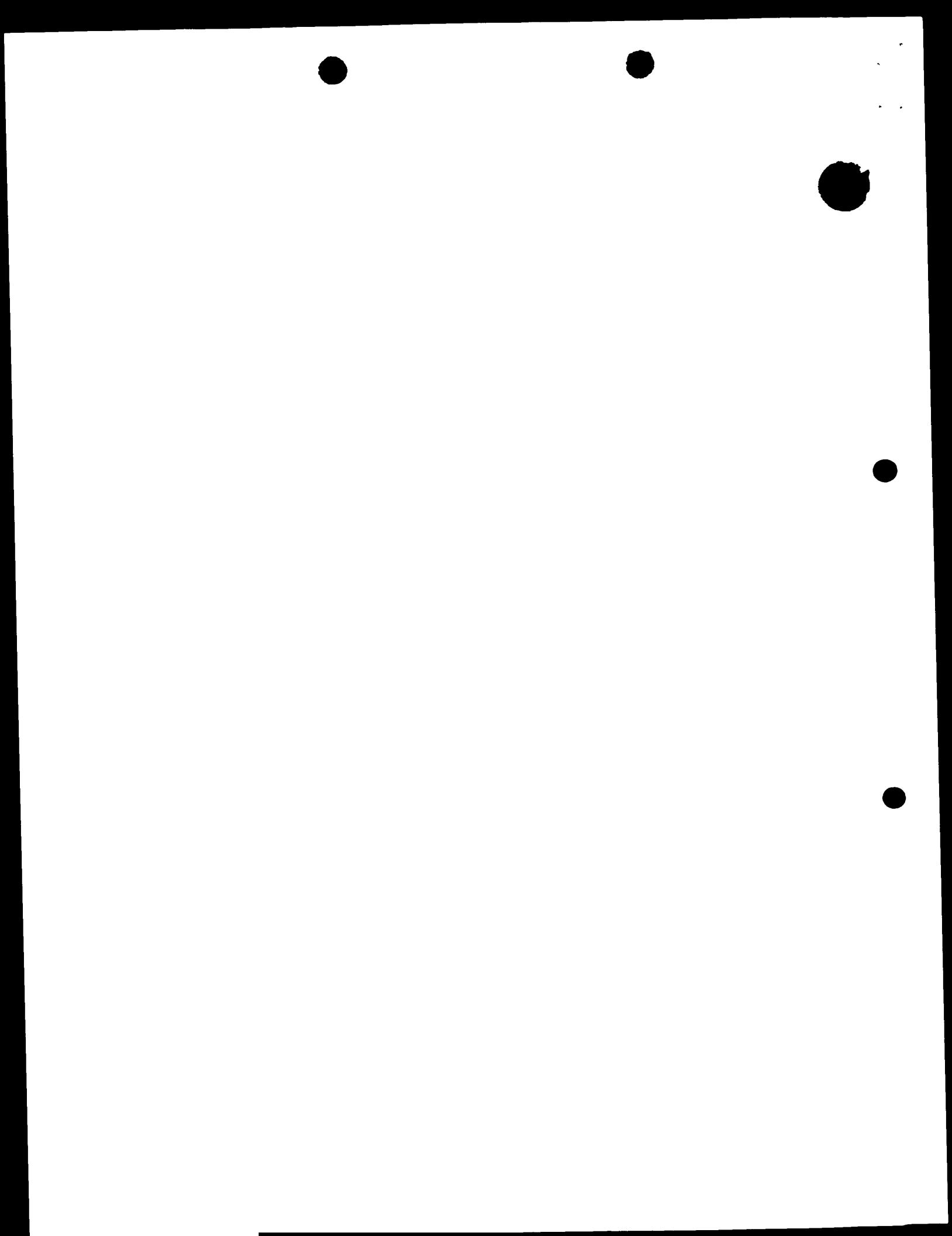


FIG 4







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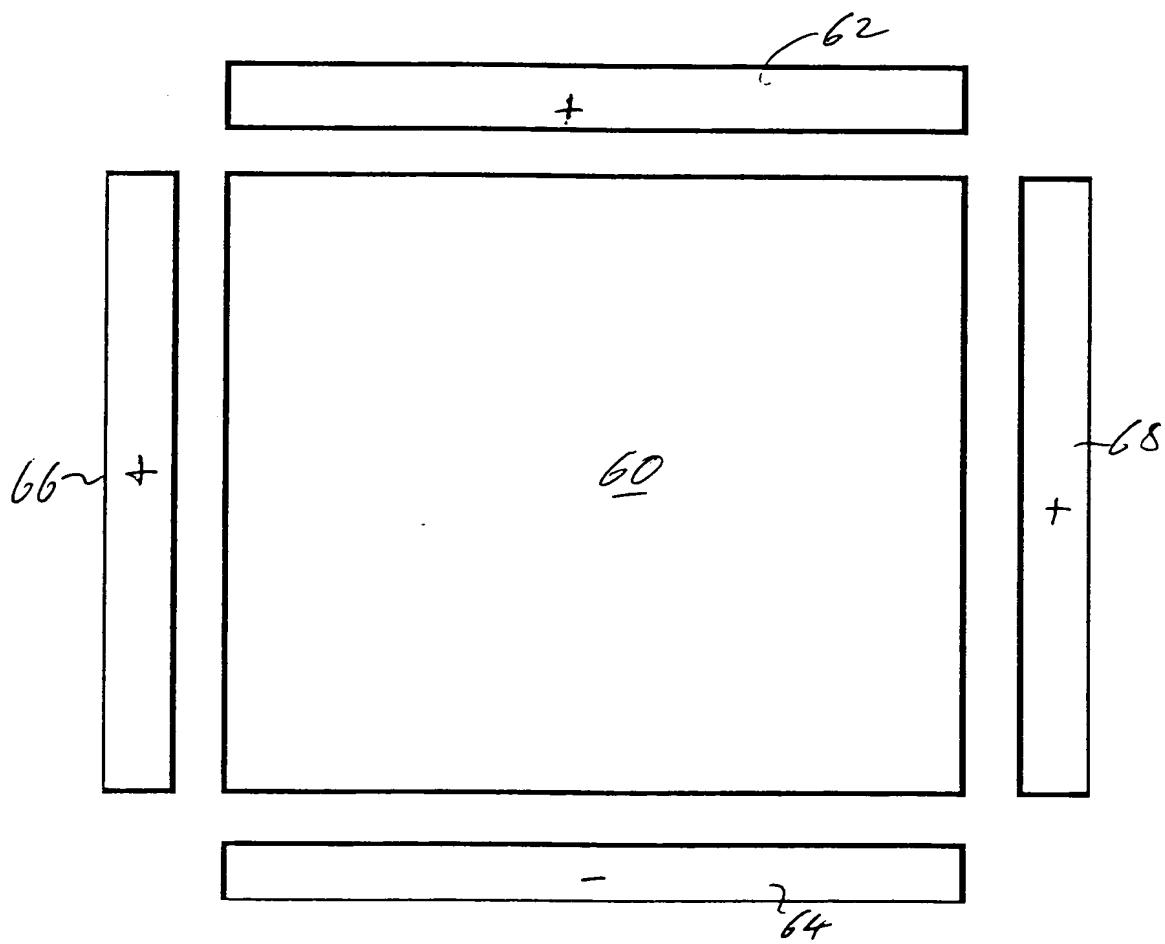


FIG 6

